

Enhanced Detection of 3D Brain Tumors through a Deep Learning Approach

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Abstract: Detection and segmentation of brain tumors in magnetic resonance imaging (MRI) are essential for clinical diagnoses and therapy planning. This research is on using segmentation algorithms to improve the detection of brain cancers in MRI data. The study seeks to delineate tumor locations with high accuracy by using modern techniques, including Convolutional Neural Networks (CNNs) and U-Net architectures. The proposed method incorporates multi-modal MRI data, including T1, T2, and FLAIR sequences, to get a holistic perspective of tumor shape. Automated segmentation alleviates the manual burden on radiologists and diminishes subjectivity, providing more consistent and precise outcomes. The research contrasts conventional segmentation methods, including thresholding and region-growing, with deep learning approaches to emphasize the benefits of contemporary machine learning in attaining superior accuracy and resilience. The approach has enhanced efficacy in identifying tiny and irregularly shaped tumors, as shown by comprehensive testing on publically accessible datasets such as BraTS. Evaluation measures, such as the Dice Similarity Coefficient (DSC) and Intersection over Union (IoU), are used to assess the efficacy of the algorithms. The results highlight the efficacy of deep learning-based segmentation as a dependable instrument for medical imaging, hence enhancing diagnostic accuracy, treatment planning, and patient outcomes. Future research may investigate the integration of these segmentation outcomes with radiomics to improve tumor characterization.

Keywords: Detection and segmentation, Brain Tumor, Magnetic Resonance Imaging, Convolutional Neural Networks, Dice Similarity Coefficient, and Intersection over Union

1. Introduction

Cellular aggregates that become tumors cause these human abnormalities. Unlike benign tumors, malignant ones invade surrounding cells and cause cancer. Physicians may struggle to manually identify these abnormal growths in patients.

Thus, improved technologies that can independently detect cancer in a particular body part are needed. Medical technology has transformed diagnosis and illness prediction. Recent advances in healthcare analysis include brain tumor segmentation, cardiovascular disease and stroke prediction, stroke biomarker discovery, and real-time ECG anomaly detection. Human skull abnormalities include brain tumors. Brain tumor detection is best done using non-invasive magnetic resonance imaging (MRI), which is safe for the complex and sensitive brain. These images depict three-dimensional brain scans. The skull has an unusual development, and each angle provides information. Classifying MRI images by perspective planes enhances brain cancer analysis. Brain tumor segmentation uses MRI data to accurately measure tumor size and location. Deep learning networks are being used more than manually built features to segregate an area of interest from an input image in current research. Deep learning is successful, but it needs costly data augmentation or massive amounts of annotated data.

a) Contribution

- The study shows how to separate brain tumors using three perspective planes instead of tri-dimensional volumetric photos.
- For exact real-time segmentation, U-Net should be

simplified.

- The proposed model is extensively compared to various segmentation methods.

b) Objective

- We provide a system that can autonomously identify malignant and benign pituitary tumors from brain MRIs and accurately segment the tumor location without medical intervention. Our strategy focuses on classification and segmentation. U-Net-based Convolutional Neural Networks section. U-Net's three-stage design—down-sampling (encoding), bottleneck (filtering unneeded information), and up-sampling (decoding)—resembles the letter 'U,' thus its name. This subgroup of neural networks is trained to identify each visual pixel with one of many possible labels.

2. Related Works

The idea is to combine location data from the decoding route with contextual information from the encoding path to predict aberrant region segmentation with a minimum of layers. The main usage of these neural networks is biological image segmentation [1-3]. CNNs that only convolution and max-pool are completely convolutional. A fully linked layer analyzes a flattened matrix in Multi-Layer Perceptrons (MLPs), which underpin this picture classification method. The last layer is often used as an activation layer with sigmoid or softmax functions. The brain's complex and changing architecture makes tumor detection difficult. Magnetic resonance (MR) imaging may help detect brain tumors. However, determining tumor sites may be time-consuming. Manually defining tumor boundaries and

classifying tumor types might lead to errors [4-8]. Gather all model training data first. T1C brain MRIs are used for this investigation. Magnetic resonance imaging (MRI) may enhance tumor localization by distinguishing CSF from adipose tissue [9]. Area parameters for brain tumor classification include volume, morphology, location, and direction. High production accuracy requires an accurate and genuine dataset. The dataset (mask image and tumor kind) includes the original picture, ground truth, and brain specimen [10-12]. Datasets must be prepared before training neural network models. Fixing production mode with picture enhancement Changes to picture characteristics, RGB-to-grayscale conversion, and realistic dimensionality reduction are included [13]. The U-Net model employs several parameters to distinguish tumor and non-tumor areas in each picture pixel. Semantic segmentation assigns values to pixels from preset sets. The three U-CNN Net components operate together. This includes downsampling and upsampling. These phases help the model recall the tumor's location and relationship to its surroundings.

3. Methods and Techniques

Figure 1 depicts the suggested blueprint for the system architecture

a) Dataset:

One of the most widely used datasets in the area of brain tumor segmentation is the BRATS dataset, which is used for multifunctional brain tumor segmentation. This dataset is known for its ease of availability and widespread popularity. The field of biomedical image analysis has made extensive use of this dataset, which has been the foundation for a significant amount of research that has been conducted in the years thereafter. As a result of the several significant research that have used this dataset, we decided to move elsewhere and make use of the dataset that is provided by BITE. The Montreal Neurological Institute obtained both the pre-processed and ground truth pictures for fifteen patients in the year 2010, and this collection contains both sets of data for those aforementioned people.

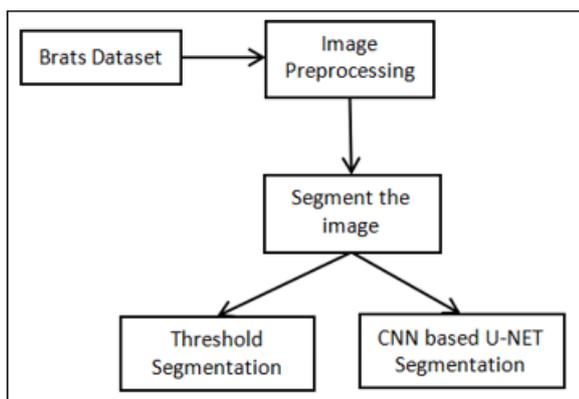


Figure 1: Proposed Architecture

b) Data Preprocessing:

MRI scans with T1 weighting and B-mode ultrasounds are used for pre-and post-surgery assessments. Neurosurgeons categorized BITE database photos into four categories based on their opinions. Our analysis focuses on 15 pre- and post-surgery MR pictures. The neuro imaging programs Nibabel

Nilearn and Python were essential for image modification and data extraction. Images were entered into Nibabel as objects and rapidly converted to NumPy arrays for image affine matrix processing. The popular Python neuro imaging program Nilearn offers MRI visualizations. Simple anatomical graphic displaying MR imaging's three dimensions. This plot may show different picture plane slices by altering the MR image's coordinates. Adjusting picture coordinates lets you construct graphs that fit its shape. Using a slice number, you may use functions to iterate across the numpy array's picture slices. Several ground truth issues may impair an algorithm's segmentation performance. The binary mask and pre-operative scan have very different resolutions.

c) Data Segmentation:

Image segmentation is a major computer vision and image processing subject with many applications. The biggest issue is matching pixels to visual elements. Many solutions have been presented for this problem. Image segmentation is common in medical imaging. Most research has modified image segmentation algorithms, especially for MRI scans, to change three-dimensional volumetric pictures. To enhance task results, these redesigned networks are tuned further. According to the computational difficulties of obtaining the ROI from the picture input, segmentation algorithms fall into four main types. These categories and algorithms will be explained in the next sections.

d) Threshold

Thresholding translates grayscale or RGB images into binary ones, making picture grouping easy. Despite its simplicity, this image ROI approach works wonderfully. Medical images were separated using the Otsu approach and global thresholding in previous investigations.

In pattern recognition, Otsu's segmentation approach is used to extract visual features for processing. This work advanced by using simple binary thresholding and the watershed approach to locate brain cancers in MRI data. Noise may degrade image quality, thus median filtering is recommended. After giving the image a binary cutoff, the watershed approach finds the key brain scan area. Small morphological modifications improve segmentation, making it more precise.

e) Deep Learning for CNN

Deep neural networks called CNNs evaluate two-dimensional pictures. Medical image analysis systems that detect health concerns use deep learning. Example: MRNet. Convolutional neural networks identify knee issues. U-Net also included three knee abnormalities network characteristics. Deep learning is used to build algorithms like this network that identify diseases from medical imaging. One of UNet's key functions is detecting the three MRI abnormalities. The network classifies output probabilities using logistic regression.

f) U-Net

Directly attached CNN U-Net does a good job at segmenting semantic images. U-Net conducts thorough analyses using its deep neural network. Benefits of image-based input data. Earth observation, consumer films, and medical imaging all

use this style. Autoencoders convert inputs into outputs in U-Nets. From input images, autoencoder networks estimate nearby data points in latent space. Data is rebuilt by compression. There are encoder-decoder routes in auto encoders. Decoders recover information from encoders by transforming it into latent space. U-Net encodes and decodes images using convolutional auto encoders. The paths for encoding and decoding are shared by U-Net and auto encoder networks. The encoder pathway of U-Net gathers

image context via convolutional and pooling layers. Using transposed convolutions, decoder path localization is accomplished. The only dense feed forward layers in U-Net are max-pooling and convolutional. Despite being initially designed for 572×572 photographs, U-Net may easily be expanded to include images of any size. The network may be able to recover valuable information from compressed Fig. 2 pictures with the use of several convolutional layers.

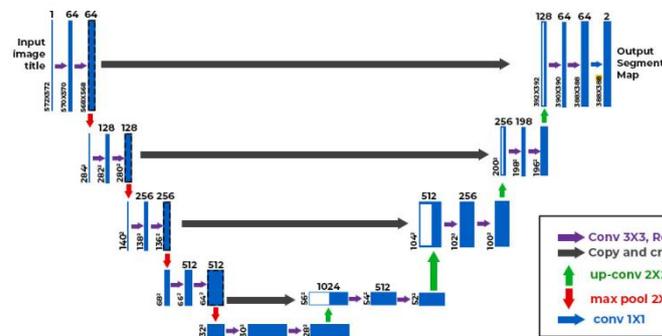


Figure 2: U-Net Architecture

4. Results and Discussion

Data about output is shared between producers and developers. Using images and kinds of tumor masks, our algorithms produce data. Select the format of the diagnostic picture. Save the little report image to your computer. Category of tumor, mask, and first picture. U-Net uses deep learning to identify tumors. The characteristics are preserved during max pooling and convolution in the three-step u-net architecture, in contrast to CNN. Decoding, bottle necking, down sampling, and encoding are the four steps involved in each phase. The properties of the encoding layer are symmetrically connected. Picture quality is preserved during copy-and-concatenation feature extraction. The pixel status of the final layer tumor region is impacted by sigmoid activation. For U-net training, small 3D datasets devoid of axial data are acceptable. To locate the tumor, many steps are used, including decoding road location and encoding route context data. A total of six data encoding blocks, one decoding block, and a single obstacle layer make up our U-Net design. For block decoding, the output layer uses sigmoid activation. We use a simple fully Convolutional Neural Network for tumor segment classification. The next three dense linear layers come after the max pooling and convolutional blocks. The soft-max activated output layer receives three output characteristics unique to tumor types from the final linear layer. A tumor-type probability vector with three elements is generated by this approach. The sort of tumor is revealed by the most probable characteristic after classification.

While testing made little use of the dataset, training made extensive use of it. You have to train the gradient with each dataset sample if you want to change the internal parameters. To enhance computing speed, it is recommended to avoid calculating the gradient for each sample. The models learned at a rate of $1e-4$ per 100 iterations. After reaching a plateau—the lack of loss reduction across two rounds—the learning rate is reduced by 0.8, removing 80% of the models. By steadily

approaching global loss minima, this method reduces overshooting. The ADAM optimizer, also known as the "ADaptive Moment," makes use of adaptive learning rates and stochastic gradient descent. The training loss matrices of both models are shown in the Matplot lib images. With its enhanced training dataset, U-Net can adapt quickly. A GeForce GTX 1660 Ti was used for training the model. Both CNN classification and U-Net segmentation took 1.5 hours. U-Net dropped 0.053 points and CNN dropped 0.138 points.

All of the BraTS multimodal scan photographs shown in Figure 4 have NIfTI files (nii.gz) accessible.

T1-weighted 2D acquisitions of the original picture taken in a sagittal or axial orientation with slices thick between 1 and 6 millimeters.

Typically, a T1c MRI scan will be performed in three dimensions with voxels that are 1 mm in size and an isotropic orientation. The scan will be gadolinium-enhanced.

2D axial T2-weighted image with 2-6 mm slice thickness representing T2.

Use a T2-weighted FLAIR picture with a slice thickness of 2-6 mm for 2D axial, coronal, or sagittal reconstructions.

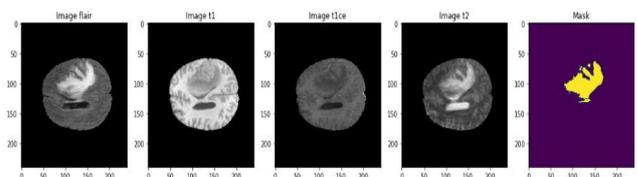


Figure 3: Shows a range of effects used to display different areas of the tumor.

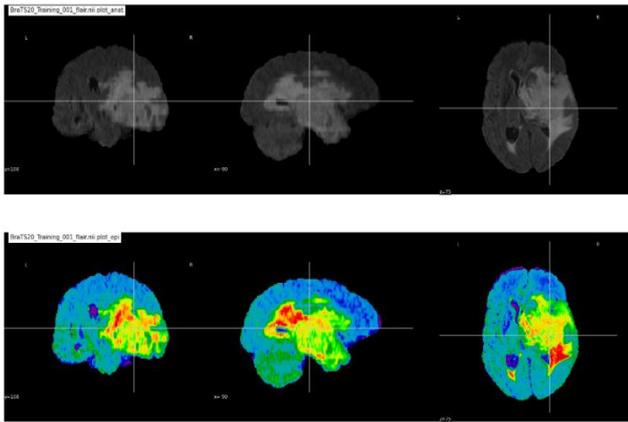


Figure 4: Different Effects of Segment Images

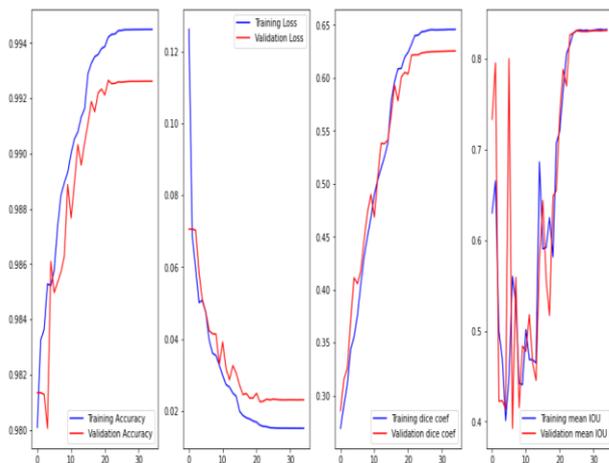


Figure 5: Imagine the steps of the training

The training and validation metrics for a machine learning model across 30 epochs are shown in Figure 5, which is a four-part image. Despite being behind the training curve, the validation curve peaks at 0.994 in the first figure, showing that both the training accuracy and validation have grown consistently. In contrast to the training loss, which stabilizes later, the validation loss drops sharply and quickly, as shown in the second line. Finally, a popular picture segmentation approach called the dice coefficient has an improvement in training and validation, but a very unstable validation line. After some volatility, especially in the validation curve, both values settle around 0.8, as shown in the fourth figure by the mean IoU (Intersection over Union). Overfitting or problematic data may explain the model's unexpected dice coefficient and IoU validation measures, despite its good learning performance.

5. Conclusion

Discovering a way to classify brain malignancies using U-Net, a deep-learning network created for biomedical image segmentation, was a major accomplishment. Following the three-dimensional flattening of MRI brain images, we searched the BITE dataset for outliers using a lightweight U-Net implementation. On one of the three viewpoint planes, the network surpasses all benchmarking methodologies and achieves an average mean IoU of 84% across all datasets. Using datasets with less than 100 photos, U-Nets' anomaly segmentation technique was tested. The lightweight U-Net technology segments data properly even

when no additional data is present. Eligible persons may get MR second opinions using this method. Given the high rate of false positives relative to false negatives in projected photographs, more investigation into a suggested network for biomedical image processing is required. The use of deep learning improves brain tumor segmentation research. We will compare our lightweight U-Net to other deep learning and statistics networks, including the original U-Net.

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